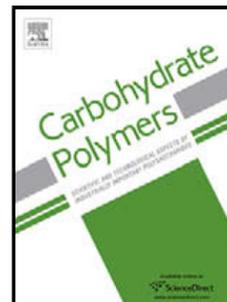


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1 A mechanism for the synergistic gelation properties
2 of gelatin B and xanthan gum aqueous mixtures

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20 **ABSTRACT:** Gelatin B and xanthan gum aqueous mixtures (GB/XG, (0.2-2%)/0.2% w/v) exhibit
21 enhanced gelling properties compared to their pure component solutions at similar compositions.
22 The mixed gels comprise co-localized networks of GB and XG-rich domains. Our results show
23 that these domains are composed of intermolecular complexes and their aggregates stabilized by
24 the neutralization effect of GB, and linked together by formation of GB triple helices. GB/XG
25 mixtures display composition-dependent microstructural transitions: from discontinuous
26 aggregates (GB/XG ratio ≤ 1) to a continuous GB/XG network (ratio = 2-6), followed by network
27 fragmentation (ratio = 8-10). Increasing the GB Bloom index accelerates network formation and
28 results in higher elastic modulus (G'), while increasing the XG molecular weight causes the
29 opposite effect due to diffusion limitations. This work provides a set of fundamental guidelines to
30 design novel thickeners and/or gelling agents based on proteins and polysaccharides, for food or
31 pharmaceutical applications.

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33 **KEYWORDS:** Gelatin, Xanthan Gum, Gelation Mechanism, Synergy, Rheology, Microstructure

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41 1. Introduction

42 Proteins and polysaccharides are two of the most important functional biopolymers in food
43 products. Their interactions in aqueous solutions can result in coacervates, complexes or gels
44 depending on charge density, protein/polysaccharide binding affinity and other molecular
45 characteristics (conformation, contour length, chain flexibility and molecular weight) (Turgeon &
46 Laneuville, 2009). These three phase states consequently exhibit different functional properties.
47 For example, protein/polysaccharide coacervates and electrostatic gels can be utilized for
48 ingredient encapsulation (Schmitt & Turgeon, 2011; Turgeon & Laneuville, 2009); complexes and
49 electrostatic gels have excellent texturing properties (Schmitt, Sanchez, Desobry-Banon & Hardy,
50 1998; Turgeon & Laneuville, 2009); and complexes can provide stabilization due to their
51 interfacial properties (Le, Rioux & Turgeon, 2016; Turgeon & Laneuville, 2009).
52 Protein/polysaccharide electrostatic gels can be formed without heat, enzyme or crosslinking
53 agents, and are therefore promising for the protection of bioactive molecules when used as
54 encapsulation and delivery systems (Le, Rioux & Turgeon, 2016; Turgeon & Laneuville, 2009).
55 In addition, they can be formed at extremely low concentrations of biopolymers (Turgeon &
56 Laneuville, 2009). In order to fully control their functional properties for application design, it is
57 necessary to understand the mechanisms involved in the interactions between proteins and
58 polysaccharides and the way in which these interactions can be tuned (Bernal, Smajda, Smith &
59 Stanley, 1987).

60 Protein/polysaccharide mixed gel formation depends on the nature and characteristics of the
61 biopolymers. For both proteins (Le, Rioux & Turgeon, 2016) and polysaccharides (Ballester,
62 Turgeon, Sanchez & Paquin, 2005), a higher biopolymer concentration is needed to form a gel
63 when the molecular weight and charge density are lower. Electrostatic forces are the dominant

64 interactions between proteins and polysaccharides in solution, but other interactions such as
65 hydrogen bonding and hydrophobic interactions can also be involved (Cooper, Dubin, Kayitmazer
66 & Turksen, 2005; Turgeon, Schmitt & Sanchez, 2007). Proteins and polysaccharides can both repel
67 and attract each other even when they carry the same net charge due to the amphiprotic properties
68 of proteins (Seyrek, Dubin, Tribet & Gamble, 2003; van der Wielen, van de Heijning & Brouwer,
69 2008; Weinbreck, de Vries, Schrooyen & de Kruif, 2003). Electrostatic forces are affected by the
70 protein/polysaccharide ratio, pH, ionic strength and biopolymer charge density (Cooper, Dubin,
71 Kayitmazer & Turksen, 2005; van der Wielen, van de Heijning & Brouwer, 2008).

72 The gelation properties of protein/polysaccharide electrostatic hydrogels are the result of a
73 delicate balance between repulsive and attractive interactions (van der Wielen, van de Heijning &
74 Brouwer, 2008; Wang, Natale, Virgilio & Heuzey, 2016). Optimal pH, protein/polysaccharide
75 ratio and ionic strength are required to tune their gelation properties. For example, our previous
76 study demonstrated that the highest elastic modulus (G') of a gelatin B (referred to here as L-GB)
77 and XG mixed gel occurs at pH 5.5 (Wang, Natale, Virgilio & Heuzey, 2016). Similarly, β -
78 lactoglobulin/XG and whey protein isolate (WPI)/XG mixtures require an optimum pH and protein
79 to polysaccharide ratio for gelation (Bertrand & Turgeon, 2007; Le & Turgeon, 2013; Sanchez,
80 Schmitt, Babak & Hardy, 1997).

81 We have also shown that GB/XG aqueous mixtures exhibit time-dependent, pH sensitive
82 synergistic gelation properties (Wang, Natale, Virgilio & Heuzey, 2016). The objective of this
83 work is to investigate the effects of composition, GB Bloom index and XG molecular weight on
84 the rheological properties and microstructure of GB/XG aqueous mixtures, in order to elucidate
85 the mechanism behind the synergistic gelation of this specific protein/polysaccharide pair.

86 **2. Materials and methods**

87 2.1 Materials

88 Two grades of gelatin (type B), G6650 (Bloom index = 75, M_w = 20-25 kDa, critical gelling
89 concentration $c_{crit} \approx 4.0$ % w/v) (L-GB) and G9382 (Bloom index = 225, M_w = 50 kDa, $c_{crit} \approx 2.0$
90 % w/v) (H-GB) were purchased from Sigma-Aldrich, Canada. Four grades of xanthan gum (XG)
91 were used: one grade (G1253) was purchased from Sigma-Aldrich Canada (the grade used in our
92 previous work (Wang, Natale, Virgilio & Heuzey, 2016), referred to here as R-XG), while the
93 other three grades with different viscosities (see Figure S1), i.e. Keltrol SF (Low-XG), Keltrol
94 (Med-XG) and Keltrol AP (High-XG), were kindly supplied by CP Kelco U.S., Inc. Other
95 chemicals (HCl, NaOH, Nile Blue A and 5-(4,6-dichlorotriazinyl) aminofluorescein) were of
96 analytical grade (Sigma Aldrich, Canada), and used as received.

97 2.2 Preparation of GB, XG and GB/XG solutions

98 GB solutions (0.4-4.0 % w/v) were prepared by allowing GB powder to swell in Milli-Q water
99 (18.2 Ω) for 15-20 min at room temperature, followed by gentle stirring at 60 °C for 15 min. XG
100 solutions (0.2 and 0.4 % w/v) were prepared by dissolving the powder into Milli-Q water at a
101 magnetic stirring speed of 600-700 rpm for at least 12 h at room temperature. Mixed GB/XG
102 solutions with a fixed XG concentration (0.2 % w/v) and different GB concentrations (0.2-2.0 %
103 w/v) were prepared by mixing equal volumes of GB and XG primary solutions, with magnetic
104 stirring, at 60 °C for approximately 30 min. The pH of the mixtures was adjusted using 1M HCl
105 or NaOH to the desired values.

106 2.3 Zeta potential measurements

107 Zeta potential values of GB and XG solutions were determined by laser doppler velocimetry and
108 phase analysis light scattering (M3-PALS) using a Malvern Zetasizer Nano ZSP instrument

109 (Malvern Instruments Ltd., Malvern, Worcestershire, UK). The zeta potential was determined
110 from the direction and velocity of the molecules in the applied electric field. The Smoluchowski
111 model was used by the software to convert the electrophoretic mobility measurements into zeta
112 potential values. All the samples were diluted to about 0.05 % (w/v) and then put into a disposable
113 folded capillary cell (DTS1060) to measure the zeta potential. The temperature of the cell was
114 maintained at 25 °C. The data presented are the average values of three individual measurements.

115 *2.4 “Table-top” rheology*

116 Small volumes (7-8 mL) of freshly prepared GB/XG mixed solutions were transferred into 20
117 mL vials (Fisherbrand, O.D. × H (with cap): 28 x 61 mm) and kept at room temperature for 24 h.
118 The vials were then inverted to qualitatively assess gel formation and strength.

119 *2.5 Time-resolved small amplitude oscillatory shear*

120 Freshly prepared GB, XG or GB/XG mixed solutions were directly poured into a rough surface
121 Couette flow geometry (cup and bob diameters of 18.066 mm and 16.66 mm, respectively) and
122 measurements were performed using a stress-controlled Physica MCR 501 rheometer (Anton Paar,
123 Graz, Austria). Before the time sweep tests, all systems were heated at a rate of 5 °C/min up to 60
124 °C. The samples were kept at this temperature for 10 min to erase the previous thermal histories
125 and were subsequently cooled down to 20 °C at a rate of 5 °C/min. Dynamic time sweep
126 measurements were performed at 1 rad/s and 20 °C in the LVE regime (strain = 3 %) for 8 h. The
127 elastic modulus (G'), loss modulus (G''), and related complex viscosity ($|\eta^*|$) were recorded as
128 functions of time. Samples were covered with a thin film of low viscosity mineral oil to prevent
129 water evaporation. The oil was shown not to affect the rheological measurements. The experiments
130 were performed at least twice with good reproducibility (< 5 %). The results of L-GB solutions

131 alone in the investigated concentration range (0.2 - 2.0 %, w/v) and of H-GB at concentrations less
132 than 1.0 % w/v were too low and noisy to be reported.

133 2.6 Confocal laser scanning microscopy (CLSM)

134 CLSM observations of the GB/XG solutions were performed with an Olympus IX 81 inverted
135 Confocal Microscope (Olympus Canada Inc., Richmond Hill, ON, Canada). GB was stained with
136 Nile Blue A (N0766, Sigma) in solution under magnetic stirring for 30 min before mixing with
137 XG solutions. On the other hand, XG was covalently labeled with 5-(4,6-dichlorotriazinyl)
138 aminofluorescein (DTAF) (D0531, Sigma) using a method described previously (Wang, Natale,
139 Virgilio & Heuzey, 2016). Preliminary experiments showed that labeling did not change the
140 rheological behavior of the solutions. After mixing, solution samples were poured into Petri dishes
141 (P35G-1.5-14-C, MatTek), which were closed with cover slips and hermetically sealed with oil.
142 Observation of XG was made by excitation of DTAF at 488 nm, the emission being recorded
143 between 510 and 550 nm. Observation of GB was made by excitation of Nile Blue A at 633 nm,
144 the emission being recorded between 650 and 680 nm. Micrographs were taken using a 60x
145 objective lens at a 2048 x 2048 pixels resolution. All micrographs were subsequently analyzed
146 using Image J software. To calculate the average size of GB-poor domains, at least 10 small bright
147 regions (50 x 50 μm) from no less than 2 different CLSM images for each sample were selected.
148 Brightness and contrast were adjusted to make GB-poor domains clearer, and the micrographs
149 were then transformed into 8-bit binary images. A median filter was used to remove noise and
150 smooth contours. By modeling GB-poor domains as cylinders, an average diameter value
151 corresponding to a microstructure length scale could be obtained (Esquirol, Sarazin & Virgilio,
152 2014; Galloway, Montminy & Macosko, 2002; Li & Favis, 2001). The calculation method is
153 briefly described next (Wang, Natale, Virgilio & Heuzey, 2016).

154 The specific interfacial area, S , between GB-rich domains and GB-poor domains is first given
155 by

$$156 \quad S = \frac{P}{A} \quad (1)$$

157 where P is the interfacial perimeter between GB-rich and GB-poor domains (obtained by image
158 analysis), and A is the micrograph area. The average diameter d of GB-poor domains is then
159 obtained as follows:

$$160 \quad d = \frac{4\Phi_{GB-poor}}{S} \quad (2)$$

161 where $\Phi_{GB-poor}$ is the volume fraction of GB-poor domains in solution, also obtained by image
162 analysis (because of microstructure isotropy, the GB-poor domains surface fraction on the
163 micrographs is taken equal to the volume fraction in solution).

164 In this work, GB-rich domains can also be referred to as biopolymer-rich domains since XG and
165 GB are mixed at pH close to the pI of GB, where strong complexation occurs.

166 *2.7 Micro-differential scanning calorimetry (Micro-DSC)*

167 Micro-DSC experiments were performed on a micro-calorimeter (Microcal Inc., Northampton,
168 MA, US) with a cell volume of 0.520 mL and under an external pressure of 180 kPa. The samples
169 were first degassed using a bath sonicator (FS110, Fisher Scientific, Pittsburgh, PA, US) operated
170 at 135 W for 30 min while heating (final temperature ≈ 80 °C), and were then injected into the
171 sample cell and kept at 90 °C for 15 min to remove any effects of thermal history. The samples
172 were subjected to cooling and heating cycles over a temperature range of 10-90 °C at a rate of 1
173 °C/min. The sample cell was cleaned by a continuous flow of hot deionized water after each
174 experiment followed by a water-water baseline test to ensure there was no contamination of the
175 sample cell. The experimental data were analyzed using the Origin-based software provided by

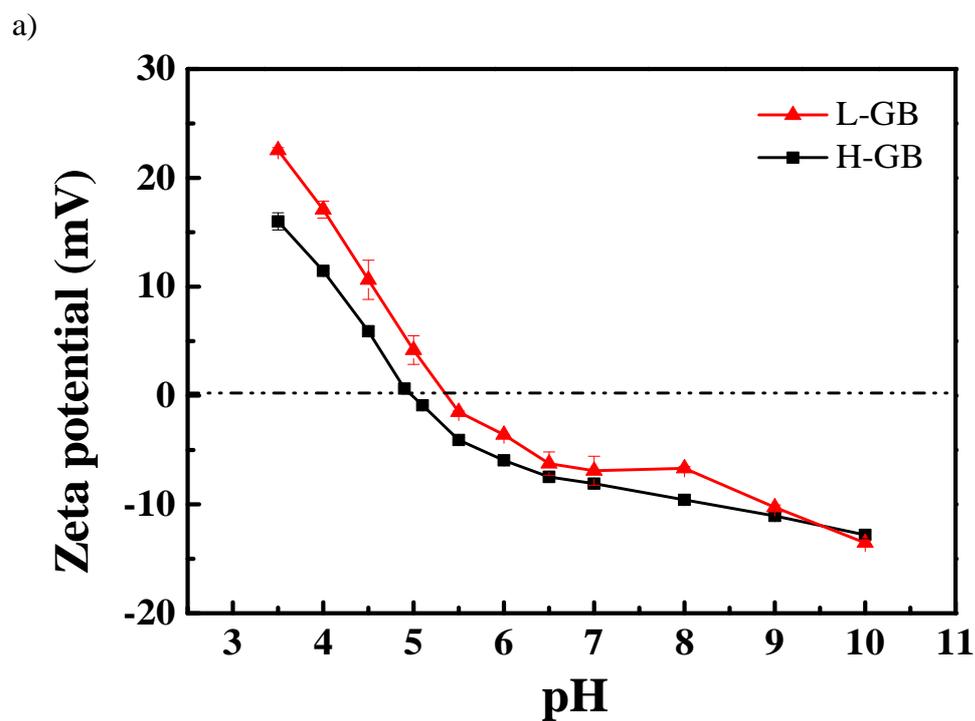
176 the manufacturer. The transition temperatures were taken at the transition peaks maxima, and the
177 transition enthalpies were determined from the area of the endothermic or exothermic peaks.

178 **3. Results and discussion**

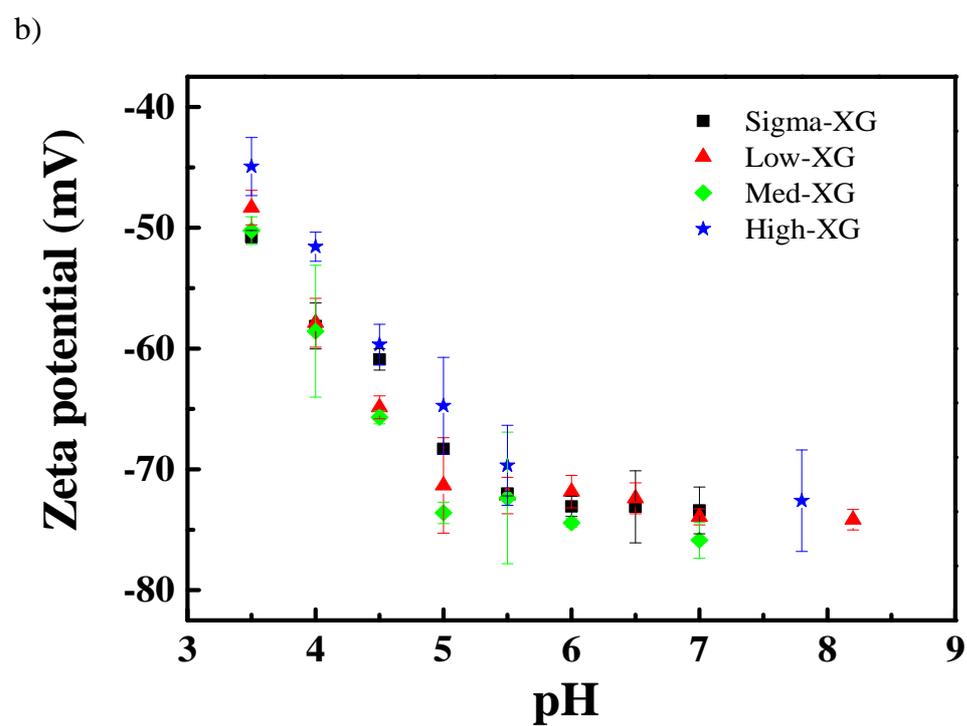
179 *3.1 Zeta potential of GB and XG*

180 **Figure 1** shows the zeta potential values of all GB and XG grades. The isoelectric point (pI) of
181 L-GB is around 5.2-5.3, which is higher than that of H-GB (≈ 4.9) (**Figure 1a**). The values agree
182 with those reported in the literature (Derkach, Ilyin, Maklakova, Kulichikhin & Malkin, 2015;
183 Williams, Phillips & McKenna, 2003), and both GB grades show positive zeta potential at pH
184 below the pI, while negative values are exhibited above the pI, indicating a change of the overall
185 charge.

186 Consistent with literature (Le & Turgeon, 2013), the different XG grades show no significant
187 difference in zeta potential values (**Figure 1b**): a strong negative dependency of zeta potential on
188 pH occurs over the range of pH 3.5-5.0. This is due to the deprotonation of -COOH groups with
189 increasing pH, and is followed by a plateau after deprotonation is complete. Note that the data for
190 R-XG were reported in our previous work (Wang, Natale, Virgilio & Heuzey, 2016) .



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Figure 1. Zeta potential values of the GB (a) and XG (b) grades used in this work.

195 3.2 “Table-top” rheology

196 The effects of pH, GB concentration, GB Bloom index and XG molecular weight on the visual
197 aspects of the GB/XG mixed gels are exhibited in **Figure 2**. The properties of GB/XG mixed gels
198 are primarily controlled by a delicate charge balance and are therefore affected by pH and GB
199 concentration. At a given XG concentration, increasing the GB content decreases the charge
200 density of XG due to complexation, which favors the eventual formation of a network. However,
201 the GB content should be carefully controlled to avoid low XG charge densities, which may reduce
202 stability and lead to aggregate formation. For example, L-GB/R-XG mixed gels become more
203 elastic with increasing L-GB concentration and as shown in **Figure 2a**, they exhibit self-supporting
204 properties at L-GB concentrations between 1.0-1.6 % w/v. At 2.0 % w/v L-GB, the system loses
205 its self-holding ability. The decrease in gelation properties is not observed by “table-top” rheology
206 when the GB concentration is close to the critical gelling concentration, as indicated by H-GB/R-
207 XG mixed gels (**Figure 2b**). Here the gels become firmer with increasing H-GB concentration at
208 a given pH.

209 Similarly, at a pH below the pI of GB, positively charged GB can interact strongly with
210 negatively charged XG. This results in phase separation via the formation of insoluble complexes.
211 At a pH equal to or above the pI of GB, complexation decreases, which makes network formation
212 unlikely. In other words, an optimal pH exists to obtain the strongest gelation properties. For
213 example, see the results for L-GB/R-XG (Wang, Natale, Virgilio & Heuzey, 2016), H-GB/R-XG
214 in **Figure 2b**, and L-GB/Low-, Med-, High-XG mixed gels in **Figure 2c**.

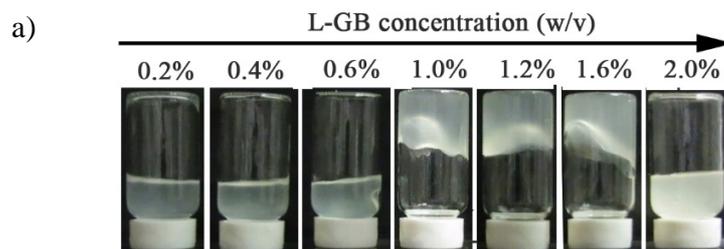
215 The “table-top” rheology (**Figure 2c**) indicates that the elastic properties decrease with
216 increasing XG molecular weight. These results also show that a synergistic gelation effect occurs

217 since the critical gelling concentration is much lower for the mixture ($c_{L-GB} = 1.0-1.6$ % w/v and

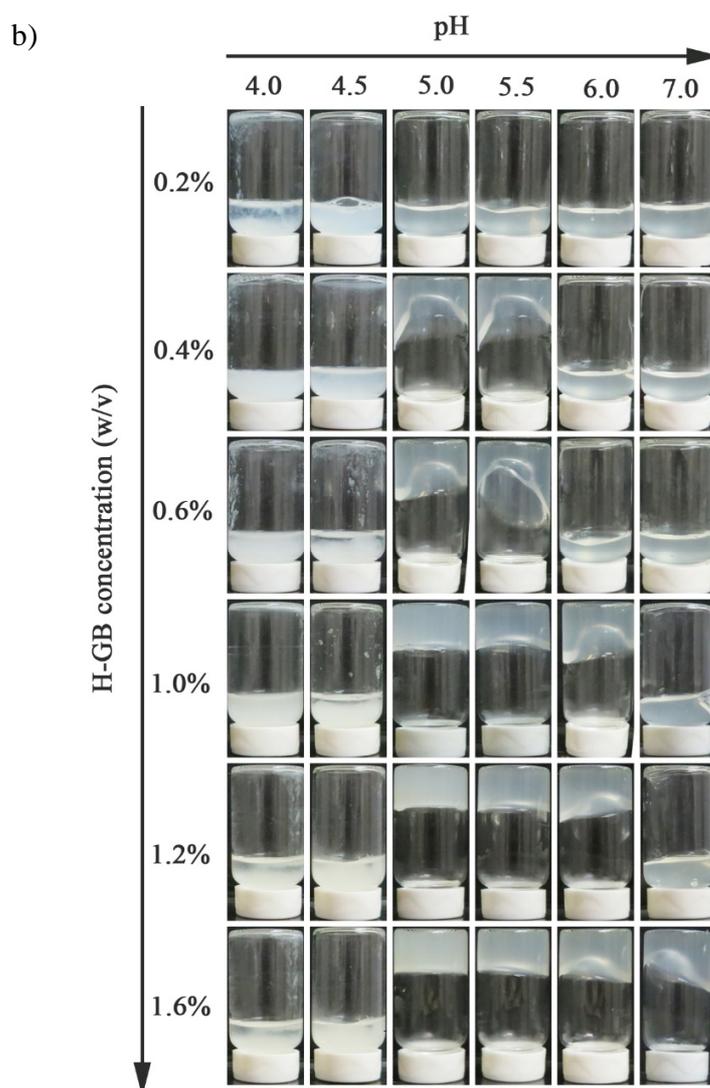
218 $c_{H-GB} \geq 0.4$ % w/v) than for GB alone ($c_{crit} \approx 4.0$ % w/v for L-GB and $c_{crit} \approx 2.0$ % w/v for H-GB).

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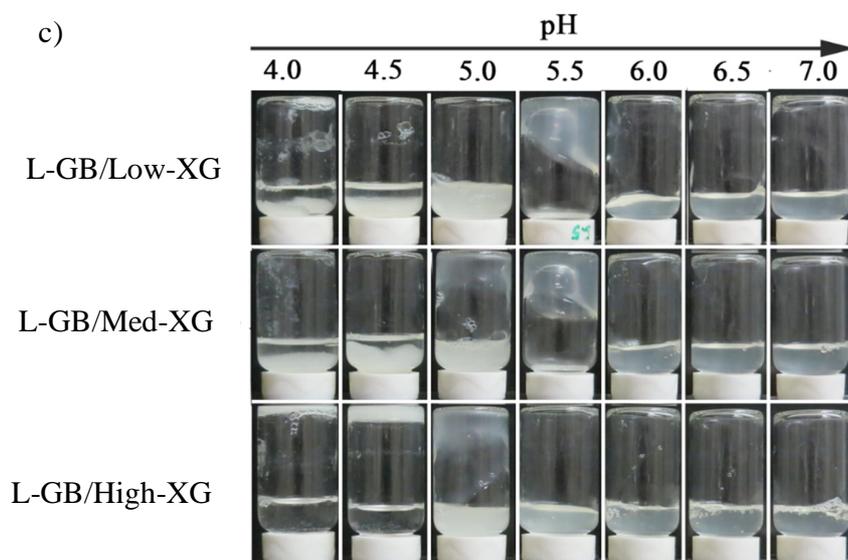
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224 **Figure 2. a) Effect of L-GB concentration ($c_{GB} = 0.2-2.0$ % w/v) on the visual aspect of L-**225 **GB/R-XG aqueous mixtures, at pH 5.5; b) effects of pH (4.0-7.0) and H-GB concentration**226 **($c_{GB} = 0.2-1.6$ % w/v) on the visual aspect of H-GB/R-XG mixtures, H-GB/R-XG ratio = 1-**227 **8; c) effects of pH (4.0-7.0) and XG molecular weight on the visual aspect of L-GB/XG**228 **mixtures (L-GB:XG ratio = 6, $c_{XG} = 0.2$ % w/v). The photos were taken after overnight**229 **storage.**230 *3.3 Time-resolved small amplitude oscillatory shear*

231 The effects of L-GB concentration and XG molecular weight on the time-dependent rheological

232 properties of GB/XG mixtures were evaluated by dynamic time sweep tests, and the results are

233 presented, respectively, in **Figure 3** and **Figure 4**. The elastic modulus (G') of the XG solution is

234 almost constant in time and always less than the values of the mixtures. The LVE properties of the

235 L-GB solutions are below the resolution limit of our instrument and are therefore not reported.

236 Mixing GB and XG significantly enhances the rheological properties and endows the system with

237 time-dependent properties. In addition, G' is always higher than G'' for these GB/XG mixtures
238 after 8 hrs (**Figure 3b** and **Figure S2**), showing a soft solid-like behavior.

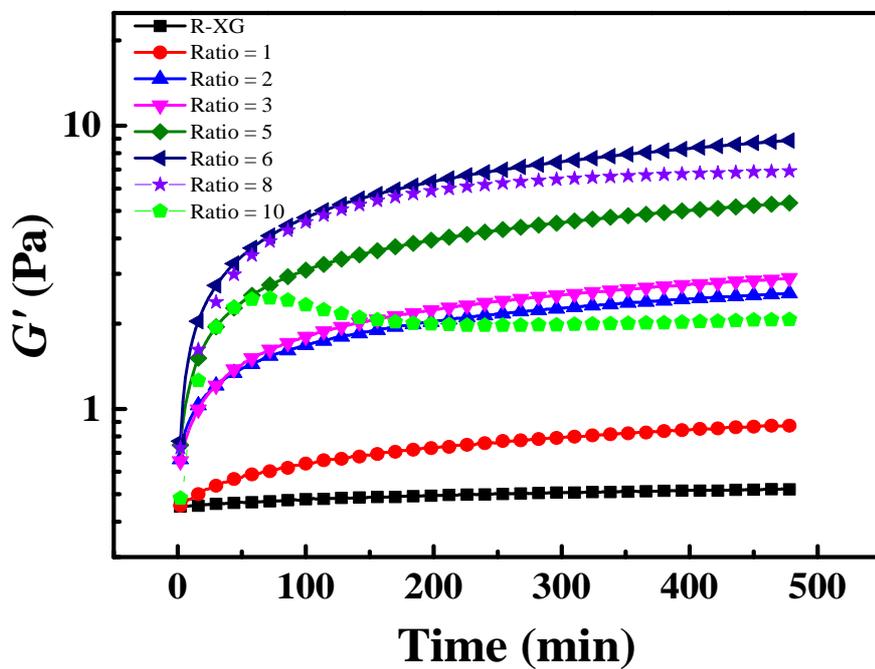
239 The G' of the mixtures initially increases rapidly followed in most cases by a slow rise, as shown
240 in **Figure 3a**, **Figure 4** and **Figure S2**. The elastic modulus after 8 hrs (G_{8h}') increases significantly
241 for the mixtures containing H-GB as compared to those containing L-GB (compare **Figure 3** and
242 **Figure S2**) but decreases as XG molecular weight increases (**Figure 4**). Note that we observe the
243 inverse effect of XG molecular weight on the initial G' (at $t = 0$ s). The mixtures show a maximum
244 G' at a certain GB concentration ($c_{L-GB} = 1.2$ % w/v and $c_{H-GB} = 1.6$ % w/v) and further increasing
245 the GB content leads to a decrease in gelation properties. These results are coherent with the “table-
246 top” rheology observations presented in §3.2.

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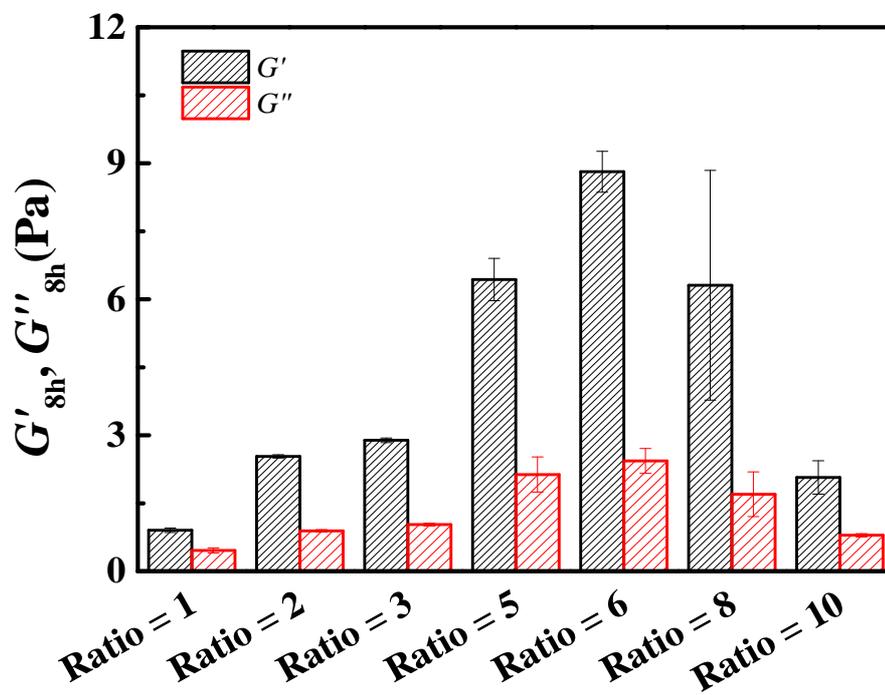
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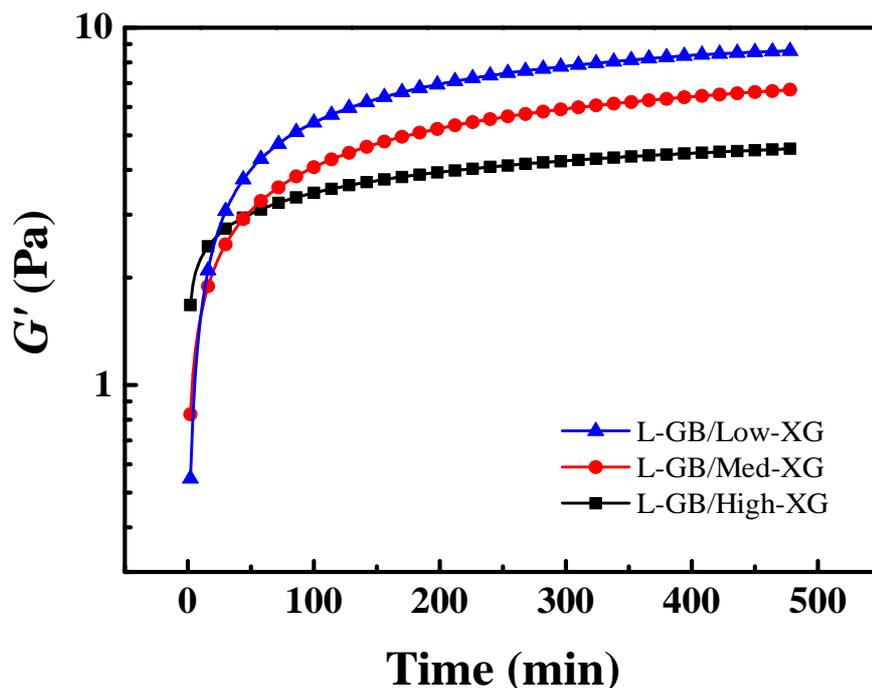
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b)



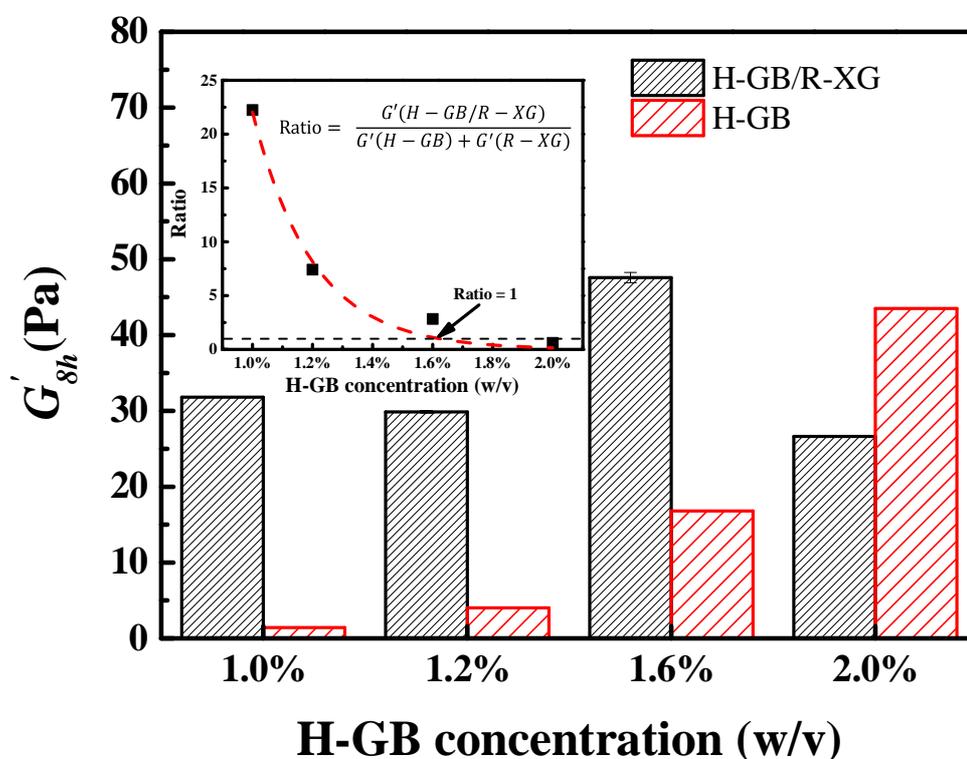
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252 **Figure 3. a) Evolution of G' as a function of time for the L-GB/R-XG mixtures at ratios (1-**
 253 **10), at pH 5.5; b) G' and G'' after 8 hrs, as a function of L-GB/R-XG ratio. $c_{XG} = 0.2$ % w/v,**
 254 $\omega = 1$ rad/s



255 **Figure 4. G' as a function of time, for the mixtures of L-GB and Low-XG, Med-XG and**
 256 **High-XG respectively, at ratio 6 and pH 5.5. XG concentration = 0.2 % w/v, $\omega = 1$ rad/s.**
 257

258 The ratios of the G_{8h}' of H-GB/R-XG mixtures, to the sum of the G_{8h}' of neat H-GB and R-XG
 259 solutions at the concentrations in the corresponding mixtures, were calculated to better evaluate
 260 the synergistic effects and are presented in **Figure 5**. This ratio is 22.2 at a GB/XG ratio of 5 (c_{GB}
 261 = 1 % w/v and $c_{XG} = 0.2$ % w/v), and decreases exponentially as GB concentration increases,
 262 clearly showing a weakening synergistic effect when the ratio ≥ 5 . The H-GB/R-XG mixture even
 263 shows a lower G_{8h}' than H-GB alone at ratio GB/XG ratio of 10, showing antagonist or detrimental
 264 gelation properties.



265

266 **Figure 5.** Comparison of G'_{8h} of H-GB solution with and without R-XG after 8 hrs in the
 267 rheometer at 20°C, $\omega = 1$ rad/s, $c_{XG} = 0.2$ % w/v. The insert shows the ratio of the G'_{8h} of H-
 268 GB/R-XG mixtures over the sum of the G'_{8h} of neat H-GB and R-XG at concentrations in
 269 the corresponding mixtures, as a function of H-GB concentration.

270 In the next section, confocal laser scanning microscopy is employed to analyze the
 271 microstructure of the mixtures.

272 3.4 Confocal laser scanning microscopy (CLSM)

273 **Figure 6** shows a set of images for L-GB/Sigma-XG mixtures at different ratios, while **Figure**
 274 **7** exhibits the effect of XG molecular weight on L-GB microstructure. The microstructure of
 275 GB/XG mixed gels generally consists of biopolymer-rich and biopolymer-poor domains. In

276 comparison, neat GB and XG solutions at similar concentrations have no visible structure and
277 appear homogeneous (images not shown). Both GB and XG exhibit a composition-dependent
278 structural transition in mixed gels. GB has a discontinuous agglomerated morphology at low GB
279 content ($c_{GB} \leq 0.2$ % w/v); a continuous network structure at intermediate GB content followed by
280 a fragmented network structure at high GB content ($c_{L-GB} = 1.6$ % w/v and $c_{H-GB} = 2.0$ % w/v).
281 This is seen in the left column of **Figure 6**, **Figure 7**, **Figure S4** and **Figure S5**. No XG structure
282 is observed at GB concentrations of 0.2-0.6 % w/v, but a network structure appears when the GB
283 concentration ≥ 1.0 % w/v (middle column of **Figure 6**, **Figure S4**). In this composition range the
284 biopolymer-rich domains consists of GB-rich domains colocalized with XG-rich domains (right
285 column of **Figure 6**, **Figure S4**). For the systems with GB/XG ratios of 5 and 6 we observe
286 significant XG content in the biopolymer-poor domains whereas at higher ratios most of the XG
287 appears to be colocalized with the GB-rich domains. The biopolymer-rich domains first decrease
288 in size (up to ratio 6) and then grow again (ratio ≥ 8) with increasing GB concentration. As we
289 reported previously, the XG network disappears when increasing the pH to 7.0 (**Figure S5**),
290 probably due to the stronger electrostatic repulsion between the molecules (Wang, Natale, Virgilio
291 & Heuzey, 2016).

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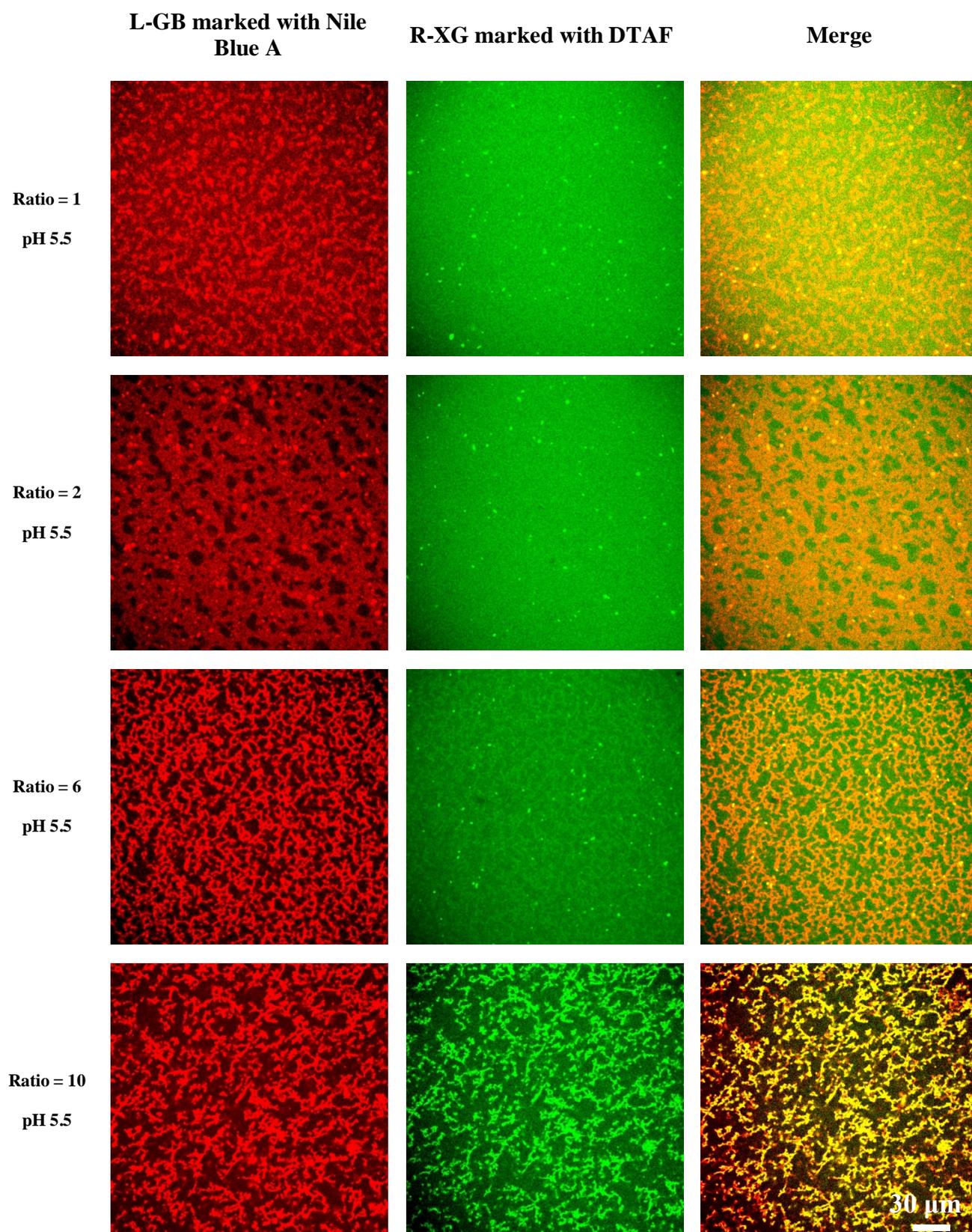
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299 **Figure 6. Microstructures of L-GB (red) and R-XG (green) domains in the mixtures at**
300 **different ratios (1, 2 6 and 10) and merge of the two imaging, at pH 5.5. The images were**
301 **taken after storage for 24 hrs. Image size: 210 μm x 210 μm .**

302 Increasing GB Bloom index leads to much finer microstructures (compare **Figures 6** and **Figure**
303 **S5**), whereas increasing XG molecular weight reduces the connectivity of the co-localized
304 networks at ratio 6, finally leading to a granular microstructure (L-GB/High-XG) (**Figure 7**).

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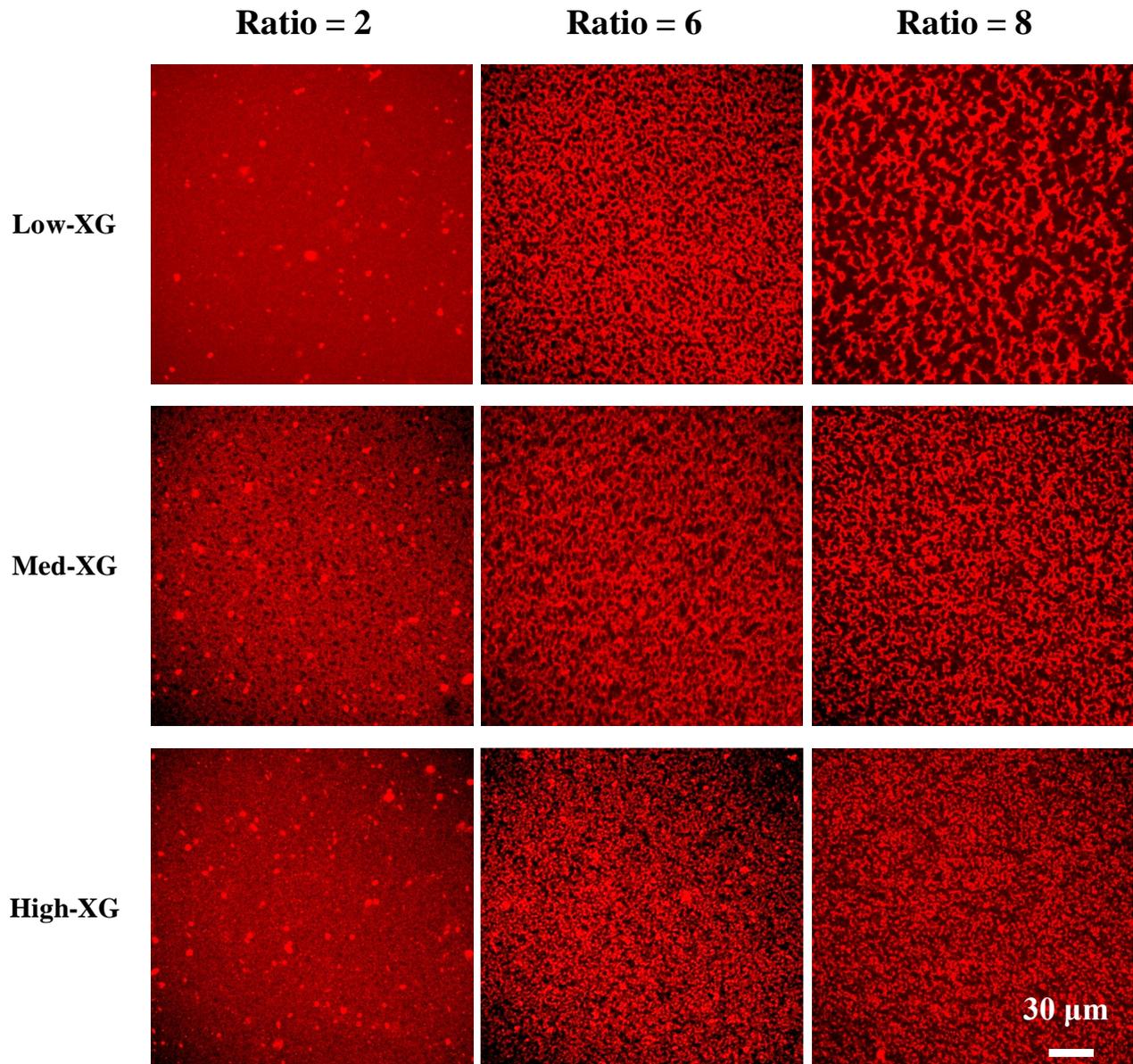
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322 **Figure 7. Microstructure of L-GB (red) when mixed with Low-XG, Med-XG and High-XG,**
 323 **respectively, at different ratios (2, 6, and 8) and pH 5.5. The images were taken after**
 324 **storage for 24 hrs at room temperature. Image size: 210 μm x 210 μm .**

325 By modeling biopolymer-poor domains as cylinders, an average diameter value $d_{\text{biopolymer-poor}}$ can
 326 be calculated, corresponding to a characteristic microstructural length scale (Esquirol, Sarazin &
 327 Virgilio, 2014; Galloway, Montminy & Macosko, 2002; Li & Favis, 2001; Wang, Natale, Virgilio

328 & Heuzey, 2016). The results are shown in **Figure 8**. The average size of biopolymer-poor
329 domains increases with GB content. The biopolymer-poor domain size is always higher for L-
330 GB/R-XG gels as compared to that of H-GB/R-XG gels.

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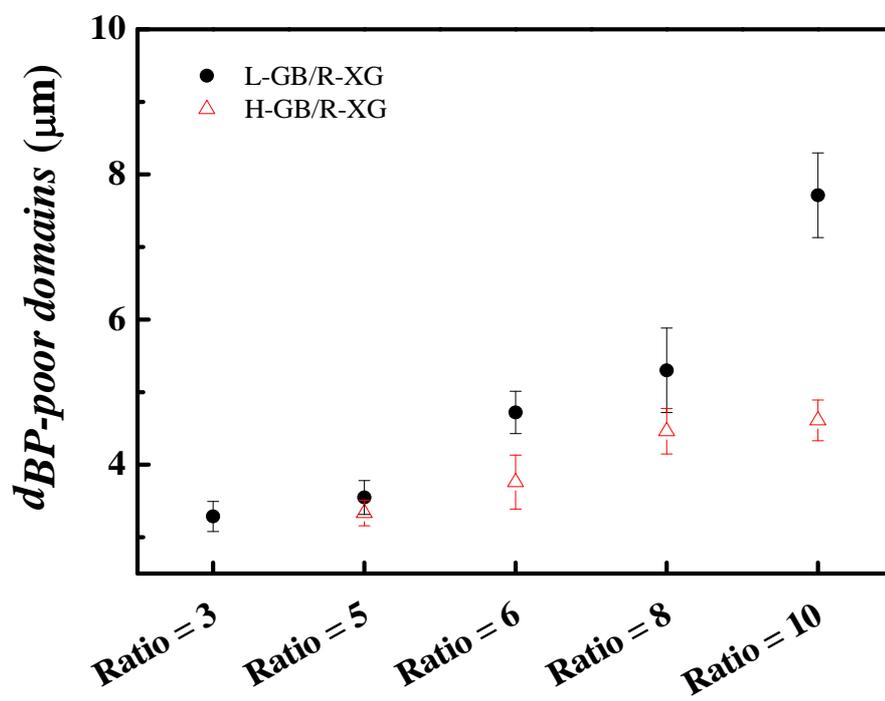
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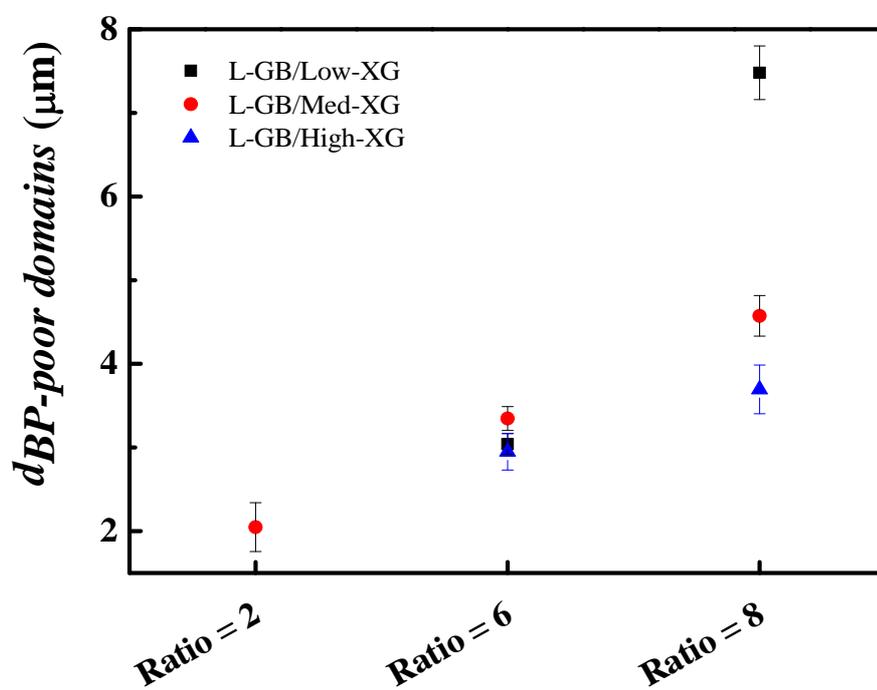
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a)



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b)



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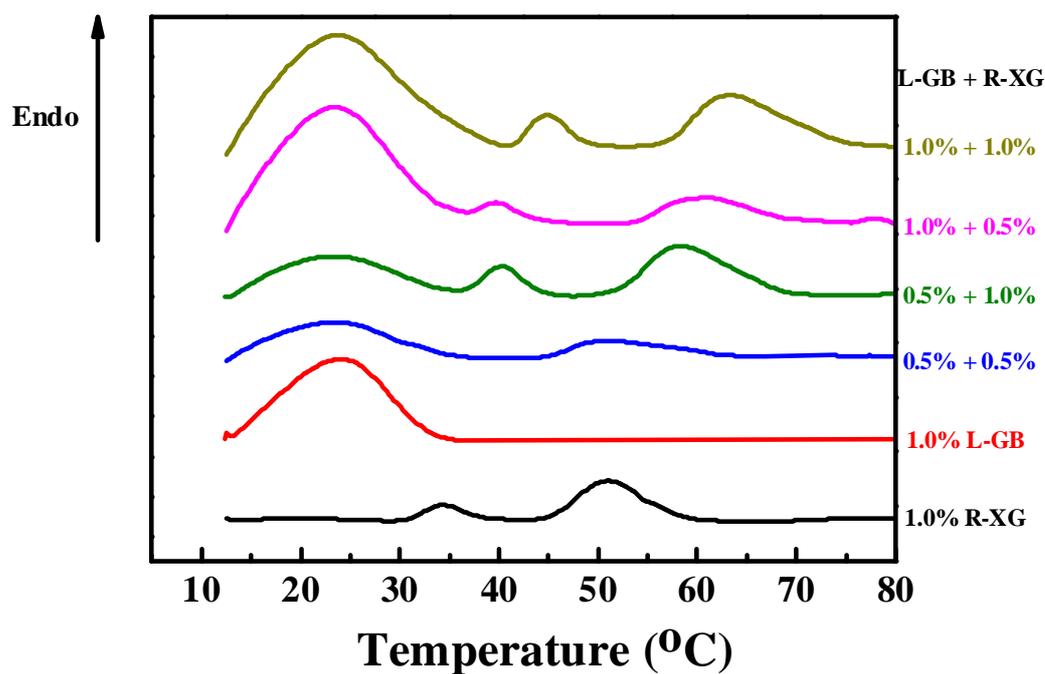
342 **Figure 8. a) Average size of biopolymer-poor (BP-poor) domains in L-GB/R-XG and H-**
343 **GB/R-XG mixtures, as a function of GB/R-XG ratio; and b) average size of biopolymer-**
344 **poor domains in L-GB/Low-XG, L-GB/Med-XG and L-GB/High-XG mixtures, as a**
345 **function of L-GB/XG ratio.**

346 *3.5 Micro-calorimetry*

347 Micro-DSC is a powerful technique to study the helix-to-coil (order-to-disorder) transition of
348 polysaccharides and proteins, such as XG (Fitzpatrick, Meadows, Ratcliffe & Williams, 2013;
349 Fitzsimons, Tobin & Morris, 2008; Norton, Goodall, Frangou, Morris & Rees, 1984; Pelletier,
350 Viebke, Meadows & Williams, 2001), DNA (Chiu & Prenner, 2011; Sturtevant, 1987),
351 carrageenan (Liu, Huang & Li, 2016; Liu & Li, 2016) and gelatin (Alqahtani, Ashton, Katopo,
352 Jones & Kasapis, 2016; Sarbon, Badii & Howell, 2015). Here, micro-DSC was used to study the
353 R-XG and L-GB conformation transitions in L-GB/R-XG mixtures, shedding more light on the
354 gelation mechanism.

355 As shown in **Figure 9**, the R-XG solution at 1.0 % w/v exhibits two peaks located at 35.6 (T_2)
356 and 52.3 °C (T_3) in the heating cycle. The second peak is consistent with the transition temperatures
357 of 52 °C observed by Pelletier et al (Pelletier, Viebke, Meadows & Williams, 2001) and ~50 °C
358 observed by Fitzsimons et. al (Fitzsimons, Tobin & Morris, 2008). This peak is therefore attributed
359 to the XG order-to-disorder (helix-to-coil) transition upon heating (Fitzpatrick, Meadows,
360 Ratcliffe & Williams, 2013; Fitzsimons, Tobin & Morris, 2008; Norton, Goodall, Frangou, Morris
361 & Rees, 1984; Pelletier, Viebke, Meadows & Williams, 2001). The reason for the first peak
362 remains unknown, but it is likely related to impurities in the XG sample, as discussed at the end
363 of this section.

364 L-GB at 1 % (**Figure 9**) exhibits a peak located at 23.5 °C attributed to the gelatin helix-to-coil
365 transition (Alqahtani, Ashton, Katopo, Jones & Kasapis, 2016; Sarbon, Badii & Howell, 2015)
366 (Cheow, Norizah, Kyaw & Howell, 2007).
367



368
369 **Figure 9.** Micro-DSC heating curves, shifted vertically for clarity. Scanning rate = 1
370 °C/min.

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377 **Table 1. Specific enthalpies and transition temperatures (peak maximum) of L-GB, R-XG**
 378 **and their mixtures during the second micro-DSC heating segment.**

GB (%)	XG (%)	GB/XG ratio	Peak 1		Peak 2		Peak 3	
			T ₁ (°C)	ΔH ₁ ^a (J/g)	T ₂ (°C)	ΔH ₂ ^b (J/g)	T ₃ (°C)	ΔH ₃ ^b (J/g)
0.5	1.0	0.5	23.3	5.74	40.3	0.34	58.3	2.66
0.5	0.5	1	23.4	4.91	-	-	51.0	2.06
1.0	1.0	1	23.7	8.64	45.0	1.09	63.3	2.99
1.0	0.5	2	23.4	8.02	39.6	0.82	61.3	2.52
0	1.0	-	-	-	35.6	0.49	52.3	1.54
1.0	0	-	23.5	5.03	-	-	-	-
2.0	0	-	23.6	7.78	-	-	-	-

379 a: normalized by the mass of GB;
 380 b: normalized by the mass of XG;

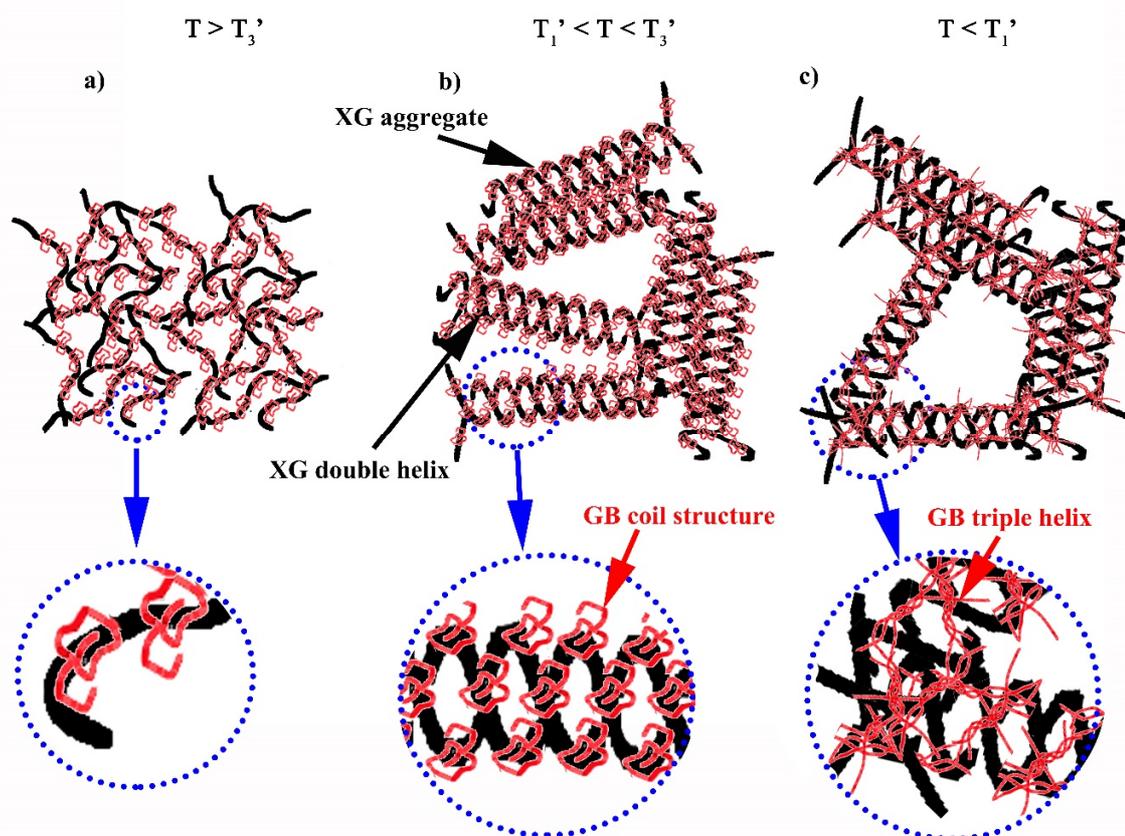
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382 The mixtures (**Figure 9**) exhibit three peaks: peak 1 corresponds to L-GB and peak 2 and 3 to
 383 R-XG. When R-XG concentration is 1.0 % w/v, the two peaks of the R-XG shift to higher
 384 temperatures in the presence of L-GB as compared to those of neat R-XG. The enthalpy of XG
 385 also increases with increasing L-GB concentration (**Table 1**). At a XG concentration of 0.5% w/v,
 386 peak 2 is no longer visible. These features indicate that more stable XG microstructures are formed
 387 with the help of GB. This phenomenon is due to the neutralization of XG molecules after
 388 complexation with GB, which then promotes the formation of the XG ordered structure.
 389 Furthermore, the enthalpy of L-GB increases in the presence of R-XG. The enthalpy values of 1.0
 390 % w/v L-GB in the mixtures are even higher than that of 2.0 % w/v L-GB alone (**Table 1**). This
 391 suggests that XG also enhances or promotes L-GB gelling by triple helix formation.

392 Note that clarified XG and its mixtures with L-GB were also studied, and they exhibit similar
393 results except that there is only one peak instead of two for the neat clarified XG, and two peaks
394 rather than three for the mixtures (see **Figure S7**).

395 *3.6 Proposed synergistic gelation mechanism*

396 XG molecules are known to undergo a disorder-to-order (coil-to-helix) transition in response to
397 charge screening and/or temperature decrease. The XG backbone takes on a helical conformation
398 and the trisaccharide side chains collapse onto the backbone and stabilize the ordered conformation
399 (Katzbauer, 1998; Rochefort & Middleman, 1987; Stephen, 1995). Weakly associated XG
400 aggregates can subsequently form side-by-side associations between neighboring ordered regions,
401 which gives a tenuous network structure and endows XG dispersions with a weak “gel-like”
402 behavior (Morris, Franklin & I'Anson, 1983; Norton, Goodall, Frangou, Morris & Rees, 1984;
403 Stephen & Phillips, 2010). Based on the properties of XG, the results above and previous
404 observations (Wang, Natale, Virgilio & Heuzey, 2016), a mechanism is proposed to explain the
405 synergistic gelation behavior displayed by GB/XG mixtures (**Figure 10**).



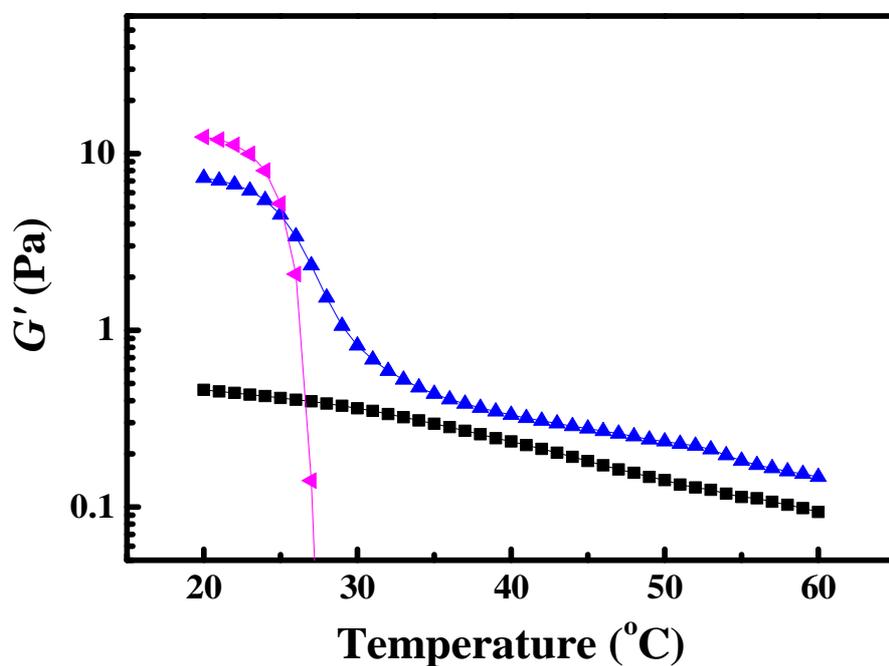
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407 **Figure 10. Proposed gelation mechanism in GB/XG mixtures, based on their interactions**
 408 **and molecular conformations.**

409 When mixing the two biopolymers in aqueous solution near the pI of GB, and above the coil-to-
 410 helix transition temperature of XG (represented by T_3'), the electrostatic attraction between the
 411 negative charges of XG and the positive patches of GB gives rise to soluble GB/XG complexes
 412 (**Figure 10a**). This complexation decreases the XG charge density. When the temperature is in-
 413 between T_3' and T_1' (representing the coil-to-helix transition of GB), the soluble complexes
 414 assemble into interpolymer complexes in the form of XG ordered structures (**Figure 10b**). Since
 415 factors that stabilize the ordered structure also favor the formation of XG aggregates (Norton,
 416 Goodall, Frangou, Morris & Rees, 1984; Stephen & Phillips, 2010), it is reasonable to say that

417 large scale assemblies of interpolymer complexes stabilized by GB are also formed under these
418 conditions through side-by-side associations between the ordered XG domains. The local
419 concentrations of both GB and XG are therefore increased. When the system is cooled down below
420 T_1' , GB triple helix formation occurs, promoted by its enhanced local concentration. With time,
421 GB/XG interpolymer complexes and aggregates concentrate locally in space and become linked
422 together due to GB gelling (**Figure 10c**). This finally results in a percolated network of
423 biopolymer-rich domains, explaining the observed increase in G' of GB/XG mixtures with time
424 (**Figure 3, Figure 4 and Figure S2**). When the network is heated again, the system first goes
425 through the helix-to-coil transition of GB (T_1 in **Table 1**), then through the helix-to-coil transition
426 of XG (T_3 in **Table 1**), since the process is reversible.

427 The proposed mechanism is further supported by a rheological temperature sweep (**Figure 11**).
428 Starting at 20 °C, when the temperature increases, we can clearly observe the helix-to-coil
429 transition in the 4.0 % L-GB system at ~25 °C, while no such features are evident in the case of
430 0.2 % w/v R-XG due to the low concentration. However, we do see the helix-to-coil transition at
431 around 52 °C if the R-XG concentration is increased to 1 % w/v (**Figure S8**), which is consistent
432 with the micro-DSC results (**Figure 9 and Table 1**). For the mixture, we observe the helix-to-coil
433 transition of the GB at just above 25 °C with the characteristic drop in the G' . This demonstrates
434 that the viscoelastic properties of the GB/XG gels, are mainly the result of the GB network up to
435 about 30 °C.



436

437 **Figure 11.** Evolution of G' during heating of three systems: (▲) L-GB = 4.0 % w/v, (▲) L-
 438 GB/R-XG = 6, total concentration = 1.4 % w/v and (■) R-XG 0.2 % w/v. Heating rate: 0.2
 439 °C/min

440 4 Conclusion

441 A gelation mechanism is proposed for gelatin B (GB)/xanthan gum (XG) aqueous mixtures.
 442 Soluble GB/XG complexes form near the isoelectric point of GB, above the coil-to-helix transition
 443 temperature of XG, followed by a disorder-to-order transition of XG due to the GB neutralization
 444 effect when the temperature is in-between the coil-to-helix transition temperature of XG and GB.
 445 The two biopolymers are locally concentrated due to the formation of large scale assemblies of
 446 interpolymer complexes stabilized by GB, and once cooled below the transition temperature of
 447 GB, a network composed of biopolymer-rich domains forms and develops over time. Increasing

448 GB concentration favors the disorder-to-order transition of XG by decreasing its charge density -
449 however, too low XG charge density destabilizes the system and results in aggregation. Therefore,
450 the GB/XG ratio must be carefully controlled to maintain the network structure and the gelation
451 properties. Stronger interactions between GB/XG interpolymer complexes when cooling down
452 leads to a faster initial evolution and higher G' , as well as a denser network. Increasing the XG
453 molecular weight decreases the mobility of soluble and/or interpolymer complexes, which then
454 weakens the concentrating effect and resulting gel properties. We are now currently investigating
455 if this mechanism applies to other protein/polysaccharide systems. This work brings a fundamental
456 understanding to the effects of proteins and polysaccharides interactions in solutions, and provides
457 important guidelines to design novel thickeners and/or gelling agents, encapsulation and delivery
458 systems.

459

460 **Supporting Information:** additional rheological results, confocal microscopy observations and
461 micro-DSC characterization.

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